

The Effect of Ferrule Design On Fracture Resistance and Failure Modes of Indirect Composite Endocrowns

Research Article

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Abstract

Objective: The effect of ferrule design on fracture resistance of endocrowns is still unknown.

Material and Methods: Thirty extracted human mandibular third molars were randomly distributed into 2 groups (n=15). In the first group, ferrule was not considered and the margins were prepared butt-joint. Second group received a circumferential 2 mm ferrule around the teeth. Conventional impressions were made. Endocrowns were fabricated of indirect composite, and then luted with resin cement. Then, all of the specimens were subjected to fracture resistance in a universal testing machine. Failure loads were recorded. Failure mode analysis was accomplished by 25x magnification optical microscope. The data were analyzed using Mann-Whitney U test, and Chi-square test ($P < 0.05$).

Results: Endocrowns with no ferrule showed a greater mean failure load (2019.69 N) than ferrule containing endocrowns (836.89 N). However, statistical analysis showed no significant difference between these two groups ($P=0.349$). Fractography analysis showed that only 4 out of 30 endocrowns exhibited catastrophic failure, and 73.3% of the failures were adhesive. And no significant difference was found between failure modes of the groups ($P=0.242$).

Conclusions: Ferrule design had no significant effect on failure loads and failure modes of endocrowns.

Keywords: Endodontically Treated Teeth; Endocrown; Fracture Resistance; Ferrule Effect.

Introduction

Prosthetic restoration of endodontically treated teeth with severe loss of coronal structure is often a clinical challenge [1], related to their higher rate of biomechanical complications when compared to vital teeth [2, 3]. They have been traditionally restored with post and cores and full crowns. [4] Despite of the clinical success using intraradicular posts, one disadvantage of using this technique is the additional reduction of sound tissue. [5] Furthermore, post-space preparation has the danger of root perforation and bacterial contamination [6]. Thanks to the advances in adhesive dentistry, endocrowns were suggested as an alternative to classical post and core approach [7]. Endocrown is a one-piece restoration which utilizes the pulp chamber surface to achieve stability and retention via adhesive bonding [8].

Endocrowns are more conservative, with much less chair time as compared to post and core technique. In addition, the functional stresses generated at the tooth/restoration interface could be better dissipated. [9] Depending on the elastic modulus of restorative material chosen, the restored tooth structure might be more rigid than the tooth (if using ceramics) or more similar to it (if using indirect resin composites) [10] Moreover, resin composites are repairable and less abrasive to opposite tooth structures in comparison to ceramics. [11]

The effect of ferrule preparation to increase the fracture resistance of crowned teeth has been well described. [12, 13] However, the incorporation of ferrule design to the endocrown preparation has not been well assessed. In most studies, [14-20] endocrowns have a butt-joint margin. And there are a few studies [21-23] which have considered ferrule design in endocrown preparation. The purpose of present study was to determine the effect of ferrule

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design on fracture resistance of indirect composite endocrowns. The null hypothesis was that there would be no difference in fracture resistance between standard endocrown restorations and the ones with a prepared ferrule.

Material and Methods

Teeth preparation

Thirty recently extracted human mandibular third molars were evaluated in this study. Teeth selection was made according to the following principles: 1. absence of caries and obvious fracture lines, 2. complete root formation, 3. approximately equal size of buccal-lingual, and mesial-distal dimensions and root length measured using digital calipers. They were stored in normal saline solution right after extraction. The roots of each tooth were coated with a layer of teflonband to simulate periodontal ligament. The specimens were then vertically mounted into auto-polymerizing acrylic resin (Repair & Pour Resin, Medidentco, Hamburg, Germany) 3 mm below the CEJ in cubical molds. Coronal structure of each tooth was removed perpendicular to its long axis approximately 2 mm above the CEJ using a slow-speed diamond saw (Isomet, Buehler Ltd, Lake Bluff, IL, USA) with water spray. Endodontic access cavities were prepared using a high-speed handpiece (NSK, Japan) and diamond burs (Tizkavan, Tehran, Iran) using copious water spray. Canal orifices were enlarged using Gates-Glidden rotary instruments (Mani, Tochigi, Japan) and pulpal tissues were removed with rotary files (DentsplyMaillefer, Ballaigues, Switzerland).

Undercuts in the access cavities were eliminated and occluso-cervical internal taper of the pulp chambers were prepared using a round-end taper diamond bur (Tizkavan, Tehran, Iran). The internal line angles were also rounded. To achieve an identical 4 mm pulp chamber depth, pulpal floors were restored using a self-cure glass-ionomer (GC, Tokyo, Japan). The teeth were then randomly divided into 2 groups (n=15). The first group did not receive additional preparation design, so margins were butt-joint 90°. The second group received a 2 mm circumferentially ferrule preparation design (Fig.1). A larger bur with the previous taper, and a finer particle size was used to polish the cervical band of the preparation. One researcher accomplished all preparations to standardize preparations.

Endocrowns Fabrication

Impressions were made using the simultaneous, dual-viscosity technique with extra light and extra heavy bodies of polyvinyl siloxane impression material (Panasil, Kettenbach, Germany) with metal stock trays. All impressions were poured in a type IV stone die (Fetwerock, Kettenbach GmbH, Germany). The separating medium was applied inside the cavity, then indirect composite (Dialog Occlusal, Rosbach, Schutz, Germany) increments were condensed and cured layer by layer to form final contour of endocrown (Fig.2). Then endocrown was removed after initial curing before final light polymerization was applied. In order to make identical occlusal form and contour of the endocrowns, an index was made from the first endocrown and used for others. Also a dental gauge was used to standardize occlusal thickness (8 mm) of each endocrown.

Cementation Procedures

The intaglio surfaces of endocrowns were sandblasted with aluminum oxide particles for 10 s. A silicone disclosing medium (Fit checker, GC, Tokyo, Japan) was used to assure proper seating of the endocrowns. Then they were cleansed in an ultrasonic cleaner (E-30H –Germany) for 5 minutes. The intaglio surfaces were etched with 37% phosphoric acid gel (Morvabon, Iran) for 10 seconds. A thin layer of silane (Pulpdent, Watertown, MA, USA) was applied with a microbrush and allowed to dry for 60 seconds. The prepared tooth surfaces were selectively etched for 20 seconds with 37% phosphoric acid gel (Morvabon, Iran), followed by water rinsing and air drying. Endocrowns were luted with a self-adhesive self-etch resin luting agent (Panavia SA Cement Plus, Kuraray, Osaka, Japan). First they were tack cured for 5 seconds using a VLC unit (ART-L3 LED, Bonart, CA, USA), and excess luting cement was removed from the margins. All surfaces then light cured for 20 seconds. These specimens were maintained in an incubator (ETUVE, Model 55.L, Pars Azma, Iran) at 37°C in 98% humidity for 24 hours.

Loading

24 hours after cementation, the fracture test was done in a universal testing machine (Zwick zo20, Germany) (Fig.3). A stainless-steel ball (3.1 mm in diameter and 0.5-m radius of curvature) with a cross-head speed of 0.5 mm per minute was applied perpendicular in the middle of the occlusal table. Force was applied until fracture. The maximum load to produce fracture was reported in Newtons (N).

Fractography

Failure mode analysis was accomplished visually by 25x optical magnification microscope (BA210E, Motic, China). Fractures were divided into 4 groups: cohesive fracture (within the endocrown material), adhesive fracture (between the endocrown and tooth), restorable tooth fracture (above the CEJ), and catastrophic tooth fracture (below the CEJ). Fracture modes were confirmed by two researchers.

Statistical analysis

Data were analyzed using a statistical software (SPSS v22.0; IBM Corp, NY, USA). In addition to standard descriptive statistical calculations (mean and standard deviation), the Mann-Whitney U-test was carried out to compare the groups, and a Chi-square test was applied for qualitative data. The statistical significance level was set at $P < 0.05$.

Results

The mean failure load of the groups is given in Table 1. According to results, the mean failure load of the no ferrule group was higher than the ferrule containing group. However, Mann-Whitney U test showed no significant differences between them ($P = 0.349$). The results of the groups' failure modes are listed in Table 2. Only 4 out of 30 endocrowns exhibited catastrophic failure, and 73.3% of the failures were adhesive. The Chi-square test revealed no significant differences between two groups ($P = 0.242$).

Table 1. Failure load results in Newton (N).

	Mean ± SD	Min	Max
Ferrule containing group	1836.89 ± 475.81	989.8	2441.16
No ferrule group	2019.69 ± 572.04	948.06	2837.74

Table 2. Failure mode results.

	Cohesive fracture	Adhesive fracture	Restorable tooth fracture	Catastrophic tooth fracture
Ferrule containing group	3 20%	10 66.7%	0 0%	2 13.3%
No ferrule group	0 0%	12 80%	1 6.7%	2 13.3%

Figure 1. Endocrown preparation: a) with ferrule, b) without ferrule.

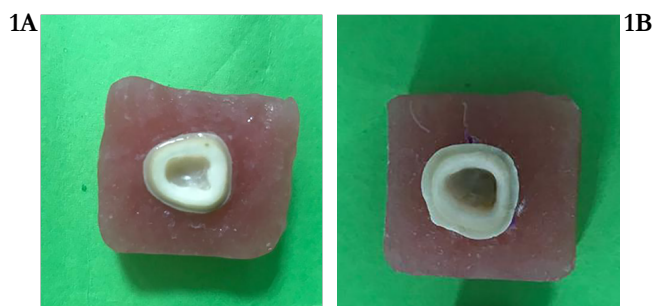
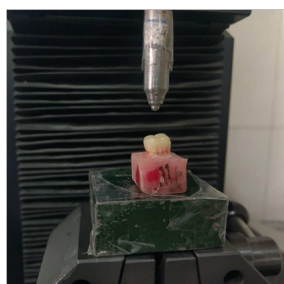


Figure 2. Indirect composite endocrown.



Figure 3. Fracture resistance testing using a universal testing machine.



Discussion

The idea of a conservative cusp coverage restoration for severely damaged endodontically treated posterior teeth is not novel. Amalgam build-ups and onlays are based on this principle. In addition to this continuum, endocrown which is an esthetic and conservative option has been newly introduced. [24]

In this study, fracture resistance of indirect composite endocrowns was investigated. The results showed no significant difference between ferrule containing and no ferrule groups which confirms the null hypothesis. So adding ferrule design to the endocrown preparation does not seem effective to increase fracture

resistance. This might be attributed to several factors. One could be due to less enamel bonding when considering ferrule design. Although, Einhorn et al [21] showed ferrule preparation could increase available surface area for adhesive bonding due to addition of available dentin surface, it has been also reported that ferrule preparation might decrease enamel and dentin for bonding, [25] which may be ascribed to a more cervical finishing line. On the other hand, endocrowns due to their greater occlusal thickness (3-7 mm) would show a higher fracture resistance to masticatory forces compared with conventional crowns. [26] Also, post core crowns consist of materials with different elastic moduli. Elastic modulus discrepancy between dentin, cement and restorative components could influence stress distribution. The more inter-

faces exist, the less stress distribution is expected. While endocrown due to its mono-block nature would support more stress loading.[27]

In most studies related to endocrown, standard preparation (no ferrule) has been used.[14-20] However there are a few studies in which ferrule preparation is considered [21-23] including the research done by Einhorn et al [21] in 2017. Contrary to the results of the present study, they showed that ferrule-containing endocrowns had significantly greater failure loads than standard endocrowns. However, computed failure stress according to the available surface area for bonding was not significantly different between the groups [21]. By considering the definition of stress as “the ratio of applied force to a cross section area (stress = F/A)”, their result might be attributed to the fact that ferrule preparation could increase available surface area for adhesive bonding. So, it seems that the numerator and the denominator of the fraction are appropriately increased.

Abdel-Aziz and Abo-Elmagd [22] recommended that the endodontically treated mandibular premolars should not be restored with endocrown in the absence of ferrule. Their study showed that presence of ferrule increased the fracture resistance of endodontically treated mandibular premolars than those without ferrule. It is inconsistent with current study result. This difference may be due to different type of teeth (premolars versus molars) used. As Bindl and Mörmann [28] evaluated the survival rate of ceramic restorations with different preparation designs cemented to premolars and molars. They observed more failures of endocrowns in premolar than molars. This would be due to the smaller size of pulp chamber in premolars, which reduces the surface for adhesive bonding.

Belleflame et al [23] evaluated 99 documented cases of endocrowns for 10 years. They reported that survival and success rates respectively were 99.0% and 89.9%. Due to the small number of failures, no statistical relationship could be found with clinical parameters like ferrule design (54.5% of cases). This result was somehow in agreement with the current study, however it should be noted that in the mentioned study only the buccal ferrule was designed. The other notable finding Belleflame et al [23] reported was that no debonding was detected on premolars, while they could be subjected to non-axial functional loading, which could result in more failures compared to molars, as revealed by Bindl et al.[28]

Lithium disilicate glass ceramic and micro hybrid resin composite materials are broadly used for indirect restorations. Microhybrid indirect composites have the advantages of lower cost and better stress-absorbing properties.[11] In this study Dialog occlusal laboratory composite was used. Mean failure load (2019.69 N) was close to the mean failure load of composite endocrowns made of Gradia (2366.50 N) and Solidex (2222.14 N) in the study by Altier et al.[29]. It should be noted that this mean failure load was well above the maximum bite force in the molars (847 N).[30]

In the study of M. Altier et al, [29] as well as Gungor et al,[31] it was shown that lithium disilicate endocrowns have higher fracture resistance than composite endocrowns. However, El Damanhoury et al [32] investigated the fracture resistance of three types of endocrowns made of lithium disilicate, feldspathic porcelain, and multiphase resin composite (Lava Ultimate). They found out

that resin composite showed higher fracture resistance than the other groups. The different results of these studies are likely due to the differences between the structures of the composites used, testing methods (diameter and velocity of piston, and angle of load application) or the cementation techniques.

In this study, there was no significant difference in failure mode between ferrule containing and no ferrule groups. Only 4 out of 30 endocrowns had catastrophic failure, and most of failures (73.3%) were adhesive. However, in Einhorn et al's study, [21] a high percentage of endocrowns catastrophically failed, regardless of the presence or absence of ferrule. This might be because of different type of material (IPS e.max CAD) used to fabricate endocrowns, and thus higher mismatch between elastic moduli of tooth and restoration.

The present in vitro study had some limitations and did not well simulate the clinical situation. For instance, thermocycling was not performed. However, in the dental literature the results on the effect of artificial aging with thermocycling on adhesion is still controversial. While some authors have not reported any significant effect, others have.[33-36] So, the clinical relevancy of such aging methods has to be confirmed in future clinical studies. Future studies are further recommended to include dynamic loading, to efficiently simulate intraoral forces.

Conclusion

Based on results of this study, there was no significant difference in failure loads and failure modes of endocrowns with or without ferrule. The mean fracture resistance of the composite endocrowns was much greater than the reported maximal bite force in molar region. And a high percentage (73.3%) of the fractures was categorized as adhesive fractures, so did not involve the tooth structure.

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